

# The case of the disappearing skull

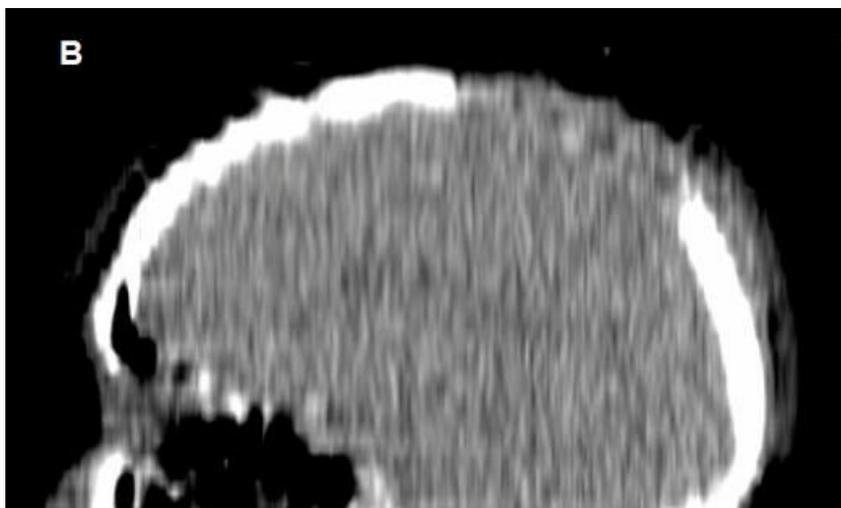
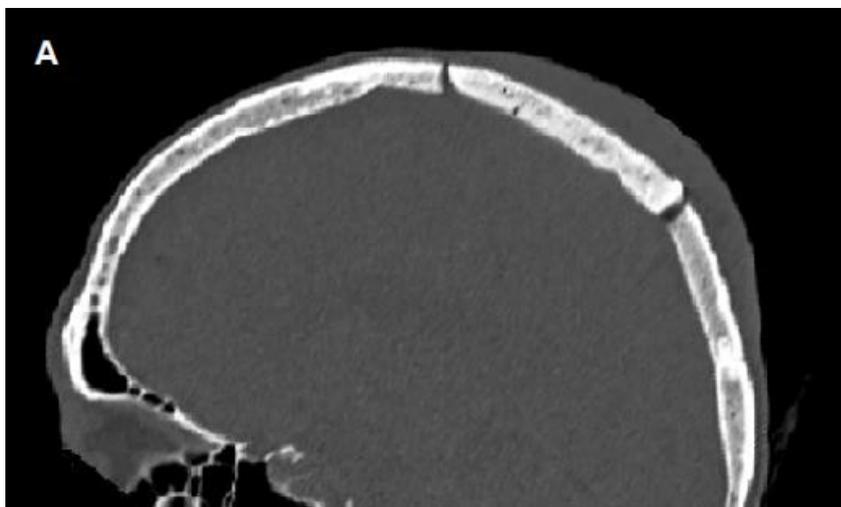
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# Setting the scene

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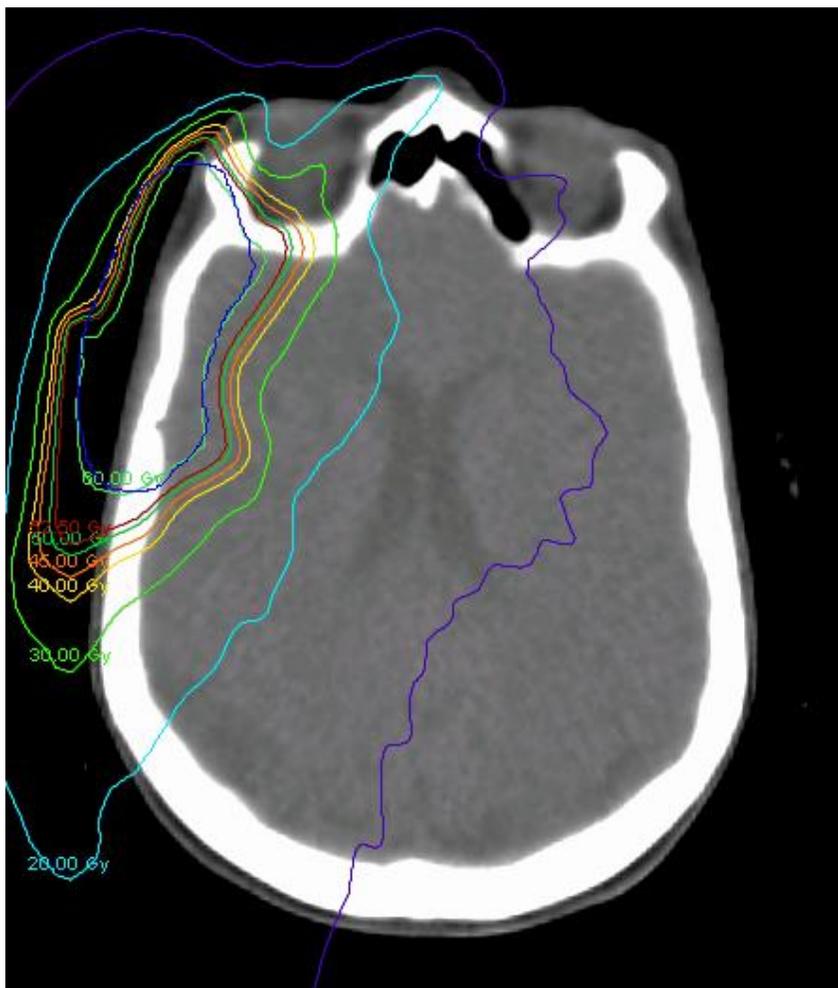
- Treatment of a scalp planned for TomoTherapy system
- “Bone flap” visible on kV CT (120 kVp)
- MVCT of patient taken on TomoTherapy system (3.5 MV), for position verification.
- **NO BONE FLAP !!!!**
- TomoTherapy planned adaptive module suggesting significant dose differences (up to 10%).



# Bone cements

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- Bone cements are used to replace bone flaps when there is involvement.
- PMMA-based cements are common, and contain radiopacifying additives, for contrast
- This is so orthopaedic surgeons can monitor the cement, e.g. to look for fractures.
- Most commonly used radiopacifiers are barium sulphate, zirconium dioxide and iodine.



# Radiological properties

- Physical cross sections for bone and bone-cement vary with energy - looking similar at 120 kVp doesn't mean they will behave similarly at treatment beam energies
- There is subsequently a risk of error in dose delivery in patients presenting with PMMA-based cements; where these additives are not appropriately handled within the treatment planning system, e.g. through the use of density overrides.

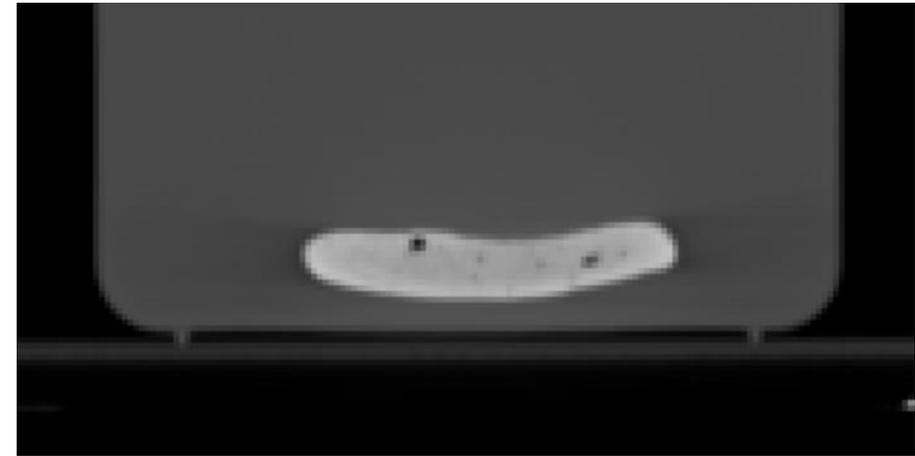
# Investigating potential errors

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- We wanted to characterize the potential dose disagreement resulting from treating a PMMA-based bone cement flap as what it appears as: bone.
- To do this, we needed to characterise the radiological properties of the material.
- We did this by:
  - Measuring effective  $\rho$  and RED ( $\rho_e / \rho_{e,w}$ ) from CT images
  - Measuring effective RED from transmission measurements / radiological thickness
  - Monte Carlo simulation of material

# CT imaging of sample

- A physical sample was secured and imaged in a small water bucket.
- ImageJ was used to obtain mean  $\pm$  standard deviation in a region of interest, not including any substantial air bubbles.
- Gammex CTED data used for  $\rho$  and RED.



Modality	Energy	CT number (HU)	$\rho$ (g/cm <sup>3</sup> )	$\rho_e/\rho_{e,w}$
Siemens kV CT	120 kVp	1100 $\pm$ 60	1.78 $\pm$ 0.04	1.66 $\pm$ 0.03
TomoTherapy MV CT	3.5 MV	50 $\pm$ 30	1.06 $\pm$ 0.04	1.04 $\pm$ 0.03

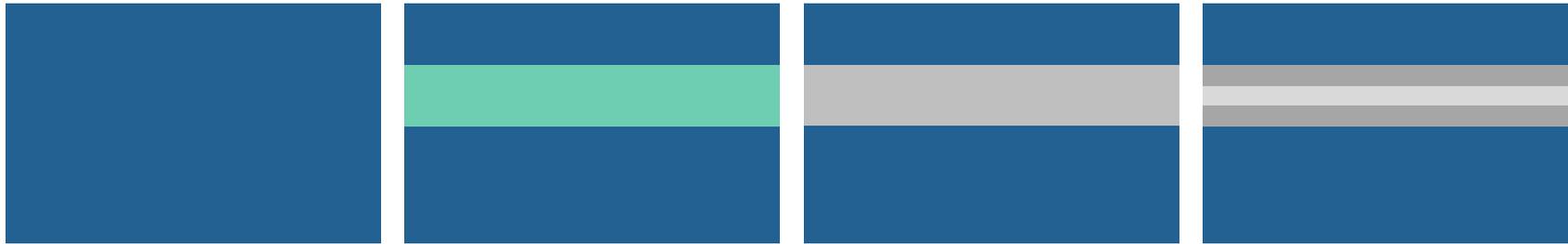
# Radiological thickness

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- Transmission measurements were performed using a TPR-type experiment geometry, i.e.
  - Fixed detector position, with 10 cm backscatter provided as possible.
  - TPR data obtained for varying thickness of virtual water.
  - TPR data obtained with bone cement added to the geometry.
  - Water-equivalent radiological thickness of the bone cement determined by interpolation.
  - Divided by the physical thickness of the bone cement sample, to obtain effective RED.

Modality	Energy	Detector	$t_w$ (mm)	$(\rho_e/\rho_{e,w})_{eff}$
WOmed T-300	100 kVp / 6.3 mm Al HVL	Roos	$25.3 \pm 1.3$	$2.5 \pm 0.1$
Varian Clinac	6 MV	Roos	$10.2 \pm 0.1$	$1.02 \pm 0.08$
Varian Clinac	6 MV	EPID	$10.9 \pm 0.8$	$1.08 \pm 0.10$

# Monte Carlo simulations



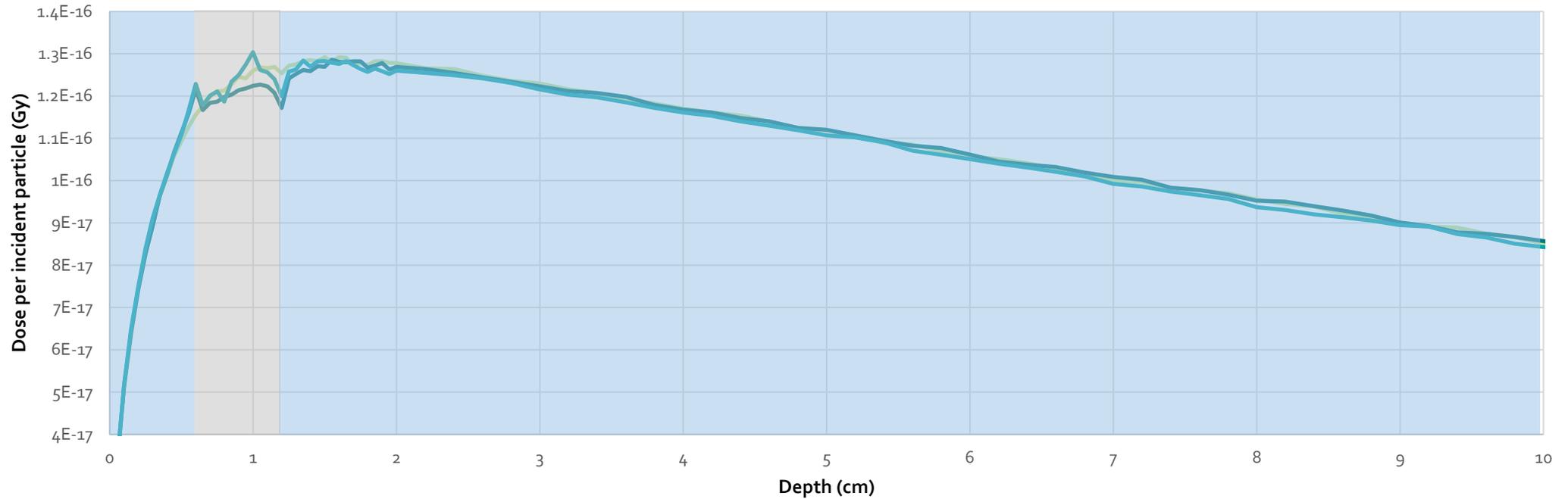
- Monte Carlo simulations were performed using known composition, for a 10 x 10 cm<sup>2</sup>, 6 MV field, 100 cm SSD.
- PDDs were produced for 4 geometries:
  - 13.2 cm water
  - 6 mm water, 6 mm bone cement, 12 cm water
  - 6 mm water, 6 mm cortical bone, 12 cm water
  - 6 mm water, 2 mm cortical bone, 2 mm spongy bone, 2 mm cortical bone, 12 cm water

Ingredient	Molecular Formula	% composition by mass
<b>Solid component (40 g)</b>		
Gentamicin sulphate	C <sub>19</sub> H <sub>40</sub> N <sub>5</sub> O <sub>11</sub> S	4.22
Polymethyl Methacrylate	C <sub>5</sub> O <sub>2</sub> H <sub>8</sub>	84.73
Benzoyl Peroxide	C <sub>14</sub> H <sub>10</sub> O <sub>4</sub>	1.95
Barium Sulphate	BaSO <sub>4</sub>	9.10
<b>Liquid component (20 ml, approx. 18.8 g)</b>		
Methyl Methacrylate	C <sub>5</sub> H <sub>8</sub> O <sub>2</sub>	98.50
N,N-Dimethyl-p-toluidine	C <sub>9</sub> H <sub>13</sub> N	≤1.50
Hydroquinone	C <sub>6</sub> H <sub>6</sub> O <sub>2</sub>	*75 ppm

# Monte Carlo results

0.6 cm water + 0.6 cm flap + 12 cm water simulation, with orthogonal incidence

— Bone cement flap    — Skull bone flap (cortical only)    — Skull bone flap (with cancellous bone)



# Conclusion

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- For beams orthogonally incident on 6 mm flaps, dose differences of 7% between bone and bone cement were observed at the interface. Given cements are usually inserted when there has been involvement (i.e. bone cement would be in / near treatment volume), this is clinically significant.
- Differences will depend on size of flap along beam axis (which may be tangential), cements with less air infiltration (which will have a reported higher HU), smaller fields.
- CT numbers produced for conventional energies (i.e. 80-140 kVp) not suitable for dose calculations, so overrides are necessary.
- Depending on air infiltration, you may not know that it is bone cement!